

## Article

# Central Nervous System: Overall Considerations Based on Hardware Realization of Digital Spiking Silicon Neurons (DSSNs) and Synaptic Coupling

Mohammed Balubaid <sup>1</sup>, Osman Taylan <sup>1</sup>, Mustafa Tahsin Yilmaz <sup>1</sup>, Ehsan Eftekhari-Zadeh <sup>2,\*</sup>,  
Ehsan Nazemi <sup>3</sup> and Mohammed Alamoudi <sup>1</sup>

- <sup>1</sup> Department of Industrial Engineering, Faculty of Engineering, King Abdulaziz University, P.O. Box 80204, Jeddah 21589, Saudi Arabia; mbalubaid@kau.edu.sa (M.B.); otaylan@kau.edu.sa (O.T.); myilmaz@kau.edu.sa (M.T.Y.); mhsalamoudi@kau.edu.sa (M.A.)
- <sup>2</sup> Institute of Optics and Quantum Electronics, Friedrich Schiller University Jena, Max-Wien-Platz 1, 07743 Jena, Germany
- <sup>3</sup> Imec-Vision Laboratory, University of Antwerp, 2610 Antwerp, Belgium; ehsan.nazemi@uantwerpen.be
- \* Correspondence: e.eftekhari-zadeh@uni-jena.de

**Abstract:** The Central Nervous System (CNS) is the part of the nervous system including the brain and spinal cord. The CNS is so named because the brain integrates the received information and influences the activity of different sections of the bodies. The basic elements of this important organ are: neurons, synapses, and glia. Neuronal modeling approach and hardware realization design for the nervous system of the brain is an important issue in the case of reproducing the same biological neuronal behaviors. This work applies a quadratic-based modeling called Digital Spiking Silicon Neuron (DSSN) to propose a modified version of the neuronal model which is capable of imitating the basic behaviors of the original model. The proposed neuron is modeled based on the primary hyperbolic functions, which can be realized in high correlation state with the main model (original one). Really, if the high-cost terms of the original model, and its functions were removed, a low-error and high-performance (in case of frequency and speed-up) new model will be extracted compared to the original model. For testing and validating the new model in hardware state, Xilinx Spartan-3 FPGA board has been considered and used. Hardware results show the high-degree of similarity between the original and proposed models (in terms of neuronal behaviors) and also higher frequency and low-cost condition have been achieved. The implementation results show that the overall saving is more than other papers and also the original model. Moreover, frequency of the proposed neuronal model is about 168 MHz, which is significantly higher than the original model frequency, 63 MHz.



**Citation:** Balubaid, M.; Taylan, O.; Yilmaz, M.T.; Eftekhari-Zadeh, E.; Nazemi, E.; Alamoudi, M. Central Nervous System: Overall Considerations Based on Hardware Realization of Digital Spiking Silicon Neurons (DSSNs) and Synaptic Coupling. *Mathematics* **2022**, *10*, 882. <https://doi.org/10.3390/math10060882>

Academic Editor: Ilya V. Sysoev

Received: 4 February 2022

Accepted: 4 March 2022

Published: 10 March 2022

**Publisher's Note:** MDPI stays neutral with regard to jurisdictional claims in published maps and institutional affiliations.



**Copyright:** © 2022 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<https://creativecommons.org/licenses/by/4.0/>).

**Keywords:** neuron; central nervous system; DSSN; brain

**MSC:** 68T07; 92B20

## 1. Introduction

In the past recent decades, a variety of mathematical computational approaches have been implemented in different research fields such as fluid mechanic engineering [1–9], chemical engineering [10–18], electrical engineering [19–28], telecommunication engineering [29–34], computer engineering [35–39], petroleum engineering [40–47], energy engineering [48–50], mathematics [51–59], environmental engineering [60–62], health and medical sciences [63–65], industrial engineering [66], etc. Among the various applied computational methods, artificial neural networks have been widely used, which demonstrates their capability. So, every effort in this field is of high importance.

Spiking Neural Networks (SNNs) are a very attractive research area based on neuronal brain cells. The time-domain field in the SNN is the main concept that is based on the

different models of neural networks. In SNNs, neurons can transmit data and information via synaptic connection, and this causes different levels of learning and memory in the human brain. In coupled neurons, when the presynaptic neuron is triggered by an applied stimulus current, this can release the voltage signals, this voltage can trigger the synaptic gap, and then the additional current is injected to the postsynaptic neurons, which is illustrated as a train of spiking behaviors in the post neurons. This behavior of neurons can be described by the spiking neuron models [67–72].

The basic elements in this system are neurons, synapses, and glia [69,73–75]. Neuron blocks are the important organs in CNS, which have several vital roles such as receiving, processing, and transmitting information to different parts of the human brain. On the other hand, synapses connect the neurons and are responsible for transferring data between neurons. Moreover, another cell called a glia can protect neurons in the CNS. Indeed, glia regulate the synaptic coupling between neurons. Thus, in the first step, the neurons' behaviors must be investigated in case of simulation and realization to obtain a compact and practical hardware.

Neurons have different behaviors and reactions. These behaviors can follow the basic pattern, which can be modeled by the mathematical equations in [76–83]. Two basic modeling systems have been presented. The first state is the biological model with biological parameters and reactions. Some basic models such as the Hodgkin–Huxley (HH) neuron model and the ADEX neuron model. These models have the biological aspects and may be a complex mathematical equation. On the other hand, SNN models are based on the spike timing patterns and less biological states. In this approach, some models such as the Izhikevic, FHN, and other models have been presented. Among these two modeling aspects, the SNN modeling may be better than the biological ones because of their low-cost implementations in hardware form. Indeed, when a compact neuron model (in hardware state) is required, the SNN models are better choices. As a result, a model named the Digital Spiking Silicon Neuron (DSSN) model is proposed [84]. This model was designed to simulate several classes of neurons by simple digital arithmetic circuits.

The implementation of different models have been realized in different positions. Two basic selections of the implementation are analog and digital states [67,68,70,71,85–90]. In analog implementation, CMOS elements are applied to achieve an analog architecture to follow the mathematical modeling of the neuron. This solution is fast, but it may suffer from long development timing. On the other hand, in the digital realization of neuronal models, a high amount of silicon may be required as well as high power consumption, but this solution can be very efficient in comparison to other methods. Some capabilities of the digital implementation are its high-degree of flexibility, reduced timing process, and power supply. In this approach, using programmable boards such as FPGAs can be very fast and flexible.

This paper presents a hardware implementation of the DSSN model in the case of a digital system. The basic challenge of this realization is the quadratic term of the original neuron model. In the general case, the quadratic term (because of its multiplier operation) causes the speed-down in the final system. In other words, in the CNS, the speed of the neuronal activity is a very important factor. If the final system does not have an acceptable frequency, it influences the neural system. Thus, this nonlinear term must be removed or converted to another simple term. Different approaches can be applied to obtain simple mathematical equations. Among these approaches, converting the quadratic terms to hyperbolic functions may be the best way. Indeed, by converting the nonlinear terms of the original model to a set of hyperbolic functions, we have a new model (by protecting all behaviors of the original mode) which converts all multiplier operations to a set of digital SHIFTS and ADDs (This method will be explained). Consequently, using the proposed new model, we have a low-cost, high-speed, and high-efficiency system which can trace the original neuron model with a high-degree of similarity and performances.

The overall method for implementing the neuronal networks can be explained. The efficient modeling, simulation, and implementation of biological neural networks are

significant. Neuromorphic engineering is a very significant subject that takes inspiration from biology, physics, mathematics, computer science, and electronic engineering to design neural systems. In the field of biology and biomedicine, the theoretical and experimental aspects of neuroscience are evaluated to have a better understanding of the brain structure. Consequently, studying, modeling, simulation, and implementing brain-like systems to realize the brain behaviors are a vital requirement. At first step, it is necessary that the neuron model is selected. In this approach, many different neuron models have been presented for spiking neural networks to reproduce their dynamical behavior. Some neuron models have biological behaviors and other models reproduce the spiking patterns of the human brain. The DSSN neuron model is a widely accepted model that can reproduce the spiking patterns of the brain. After model selection, the time domain and dynamical behaviors of the proposed neuron model have been evaluated. Indeed, the proposed model is a modified case of the basic neuron model with low-error state and low-cost hardware attributes. Since the original models have nonlinear terms and functions with high-cost realizations, it is necessary that the model is modified to a new low-cost model for its implementation on hardware platforms. To validate the proposed model in case of following the original model, spiking patterns and dynamics must be considered. These evaluations have been performed using MATLAB software simulations. Finally, to test and validate the proposed model in hardware form, we have used the FPGA system design. In fact, the Hardware Description Language (HDL) of the proposed neuron model has been considered using the ModelSim and Xilinx ISE software. In this part, the proposed model's overhead costs have been compared to the original model cost realization. The proposed model must be more efficient in comparison with the original model in case of overhead costs (overall saving in FPGA) and speed-up (maximum frequency).

This paper is organized as follows. In Section 2, the background of the DSSN model will be explained. In Section 3, the proposed procedure is evaluated. Section 4 presents the dynamic behaviors and time domain analysis. Synaptic coupling is described in Section 5. Overall hardware implementation is performed in Section 6 in detail. Production results are presented in Section 7. The limitations of the method and also future directions have been explained in Section 8. The paper concludes in Section 9.

## 2. Background

The Digital Spiking Silicon Neuron (DSSN) model is a simple practical model in terms of qualitative states. This model is capable of reproducing different classes of spiking such as Class I and Class II patterns. The DSSN model can be formulated by two coupled differential equations for voltage and recovery variables. The mathematical equations of the model are given by following statements:

$$\frac{dV}{dt} = \frac{\phi}{\tau}(f(V) - n + I_0 + I_{Stimulus}) \tag{1}$$

$$\frac{dn}{dt} = \frac{1}{\tau}(g(V) - n) \tag{2}$$

where

$$f(V) = \begin{cases} a_n(V + b_n)^2 - c_n & ; V < 0 \\ -a_p(V - b_p)^2 + c_p & ; V > 0 \end{cases} \tag{3}$$

$$g(V) = \begin{cases} k_n(V - p_n)^2 + q_n & ; V < r \\ k_p(V - p_p)^2 + q_p & ; V > r \end{cases} \tag{4}$$

In these equations,  $V$  and  $n$  represents the voltage and slow variable, respectively. On the other hand,  $V$  is the membrane potential, and  $n$  is the recovery variable for producing the voltage variable. The parameter  $I_0$  is a bias fixed parameter, and  $I_{Stimulus}$  is the applied current for neurons. The other parameters for generating the Class I and Class II patterns are presented in Tables 1 and 2, respectively. These parameters are explained as follows:

- $I_0$ : Bias constant;

- $I_{Stimulus}$ : Applied current for neurons;
- $\phi$  and  $\tau$ : Time constant;
- $r, a_x, b_x, c_x, k_x, p_x,$  and  $q_x$  ( $x = n$  and  $x = p$ ): Constants that control the nullclines of the variables (Dynamics of the model).

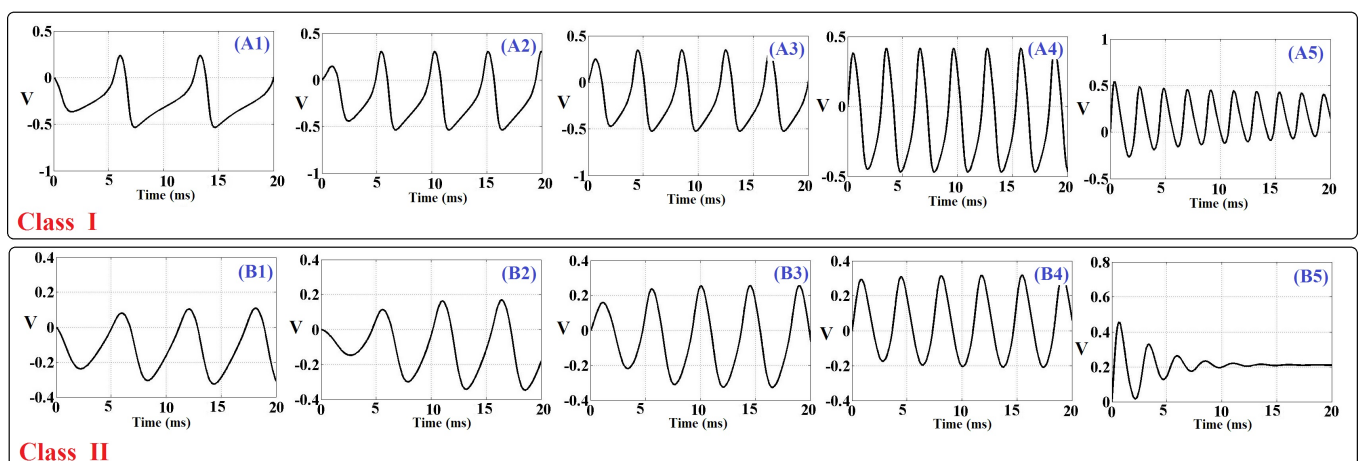
It is emphasized that the DSSN model is a spike-based neuron model, and all the variables and constants are abstracted and do not have a physical unit. In addition, by selecting appropriate values for these parameters, both Class I and Class II neurons can be realized with parameter settings. Finally, different spiking patterns based on these two basic parameters can be simulated, as can be seen in Figure 1.

**Table 1.** Different Parameters for Reproducing the Class I Pattern.

Parameter	Value	Parameter	Value
$a_n$	8	$a_p$	8
$b_n$	0.25	$b_p$	0.25
$c_n$	0.5	$c_p$	0.5
$k_n$	2	$k_p$	16
$p_n$	−0.3125	$p_p$	−0.2187
$q_n$	−0.7058	$q_p$	−0.6875
$\phi$	1	$\tau$	0.003
$r$	−0.2053	$I_0$	−0.205

**Table 2.** Different Parameters for Reproducing the Class II Pattern.

Parameter	Value	Parameter	Value
$a_n$	8	$a_p$	8
$b_n$	0.25	$b_p$	0.25
$c_n$	0.5	$c_p$	0.5
$k_n$	4	$k_p$	16
$p_n$	−0.5625	$p_p$	−0.2187
$q_n$	−1.3177	$q_p$	−0.6875
$\phi$	0.5	$\tau$	0.003
$r$	−0.1041	$I_0$	−0.23



**Figure 1.** Spike-based signals of the DSSN model. (A1–A5): Spiking patterns of Class I mode for different stimulation current as:  $I_{Stimulus} = 0.1, I_{Stimulus} = 0.2, I_{Stimulus} = 0.5, I_{Stimulus} = 1,$  and  $I_{Stimulus} = 2,$  respectively. (B1–B5): Spiking patterns of Class II mode for different stimulation current as:  $I_{Stimulus} = 0.1, I_{Stimulus} = 0.2, I_{Stimulus} = 0.5, I_{Stimulus} = 1,$  and  $I_{Stimulus} = 2,$  respectively.

### 3. Proposed Procedure

As can be seen in the mathematical equations of the original DSSN model, the basic nonlinear term of this model is the quadratic term which is repeated in all parts of the model. DSSN neuron is implemented on an FPGA digital board, but the quadratic terms of the equations cause the final system to be no more efficient. In this situation, the best method is to convert the nonlinear terms to new functions which have two basic conditions: first is the high degree of similarity between the original and proposed method and second is the low-cost digital implementation in terms of FPGA resources and higher frequency (speed-up) compared with the original DSSN model. In this approach, there are different acceptable ways to approximate and modify the original models, such as piecewise linear functions, absolute functions, and hyperbolic terms. When the original models are approximated by linear functions, the error level in the proposed model can be increased, but using the hyperbolic functions reduces the error calculation, and a high-degree of similarity will also be achieved. Thus, in this paper, we used the hyperbolic-based modifications. Another advantage of this method is that by using these hyperbolic terms, all nonlinear terms and functions in the differential equations are converted to digital SHIFTs and ADDs without any multiplications. Consequently, we have a new model with all aspects of the original model that it is efficient in terms of speed and costs compared with the original main DSSN model. In the proposed model, the equations are reformulated as follows:

$$\frac{dV}{dt} = \frac{\phi}{\tau}(F(V) - n + I_0 + I_{Stimulus}) \tag{5}$$

$$\frac{dn}{dt} = \frac{1}{\tau}(G(V) - n) \tag{6}$$

where

$$F(V) = \begin{cases} a_n(Func(V)) - c_n & ; V < 0 \\ -a_p(Func(V) - 4Vb_n) + c_p & ; V > 0 \end{cases} \tag{7}$$

$$G(V) = \begin{cases} k_n(Func(V)) + q_n & ; V < r \\ k_p(Func(V)) + q_p & ; V > r \end{cases} \tag{8}$$

where

$$Func(V) = 0.6sinh(0.65V) + 0.6cosh(1.5V) - 0.5 \tag{9}$$

In other words, based on Equations (3) and (4), when these equations are simplified, we have a new nonlinear function which is repeated in all equations. This new function can be formulated as follows:

$$NL-Func(V) = V^2 + 0.5V + 0.0625 \tag{10}$$

Consequently, this nonlinear function can be replaced by  $Func(V)$  in all parts of the original mathematical equations. By this modification, the proposed model can be implemented in low-cost and high-speed states (This procedure is elaborated in detail in the hardware section). In this approach, as can be depicted in Figure 2, the original nonlinear function ( $NL-Func(V)$ ) and the proposed hyperbolic term ( $Func(V)$ ) have a high degree of similarity, and the error level between these two equations is in the low state, which is shown in the next sections. It is noticeable that based on Figures 1 and 2, the permissible range of parameter value changes is given between  $-0.5$  and  $+0.5$ . Indeed, the modifications of the nonlinear terms of the neuron model have been conducted in this variation range.

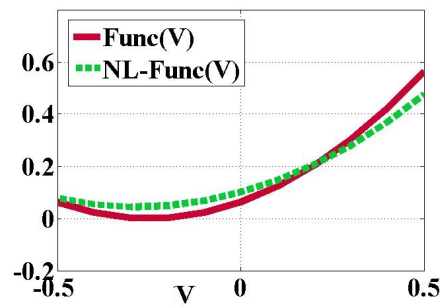


Figure 2. Approximation for the nonlinear function ( $NL-Func(V)$ ) by the hyperbolic function ( $Func(V)$ ).

#### 4. Dynamic Behaviors and Time Domain Analysis

Two basic factors should be considered for validating the proposed model. In this approach, at first, it is important that the proposed model is in the same state (as dynamical behaviors in equilibrium points and eigenvalues) as the original model; second, the time domain analysis for two models (original and proposed) is done with low error calculation.

##### 4.1. Dynamics

To investigate the modified model, the behaviors of neurons in the case of dynamics are considered. In this way, to explain the transition from resting state to spiking state (bifurcation), the interactions of the two nullclines play an important role [77,91,92].

The nullclines for the original model can be given by the following statements:

$$\begin{cases} \frac{dV}{dt} = p(V, n) \\ \frac{dn}{dt} = q(V, n) \end{cases} \tag{11}$$

$$\begin{cases} \frac{dV}{dt} = 0 ; p(V, n) = 0 \\ \frac{dn}{dt} = 0 ; q(V, n) = 0 \end{cases} \tag{12}$$

$$\begin{cases} n = f(V) - n + I_0 + I_{Stimulus} \\ n = g(V) \end{cases} \tag{13}$$

On the other hand, the nullclines of the proposed model are given as:

$$\begin{cases} n = F(V) - n + I_0 + I_{Stimulus} \\ n = G(V) \end{cases} \tag{14}$$

Consequently, for analyzing the equilibrium points, the Jacobean matrix and eigenvalues are required [77,91,92], and the Jacobean matrix can be obtained as:

$$\begin{Bmatrix} A & B \\ C & D \end{Bmatrix} \tag{15}$$

where

$$\begin{cases} A = \frac{\partial p(V, n)}{\partial V} \\ B = \frac{\partial p(V, n)}{\partial n} \\ C = \frac{\partial q(V, n)}{\partial V} \\ D = \frac{\partial q(V, n)}{\partial n} \end{cases} \tag{16}$$

According to  $J(V, n)$ , the stability of the fixed point is determined. The fixed points are stable if  $A + D < 0$ , and they are unstable if  $A + D > 0$ . On the other hand, the fixed point is stable if both of the eigenvalues of this matrix have a negative real part and is unstable if at least one of the eigenvalues has a positive real part. As can be seen in Table 3, these calculations are applied. On the other hand, Figure 3 illustrates the similarity between spike patterns of the original and proposed DSSN neuron models. As depicted in this figure, the equilibrium points are the same.

Table 3. Equilibrium Points For the Original and Proposed Models.

Point (Orig.)	Value (Orig.)	Point (Prop.)	Value (Prop.)
Saddle Point	(−0.2, −0.7)	Saddle Point	(−0.22, −0.68)
Spiral Source	(0.09, 0.92)	Spiral Source	(0.1, 0.9)
Saddle Point	(−0.28, −1)	Saddle Point	(−0.27, −0.98)
Spiral Sink	(0.24, 1.27)	Spiral Sink	(0.22, 1.25)

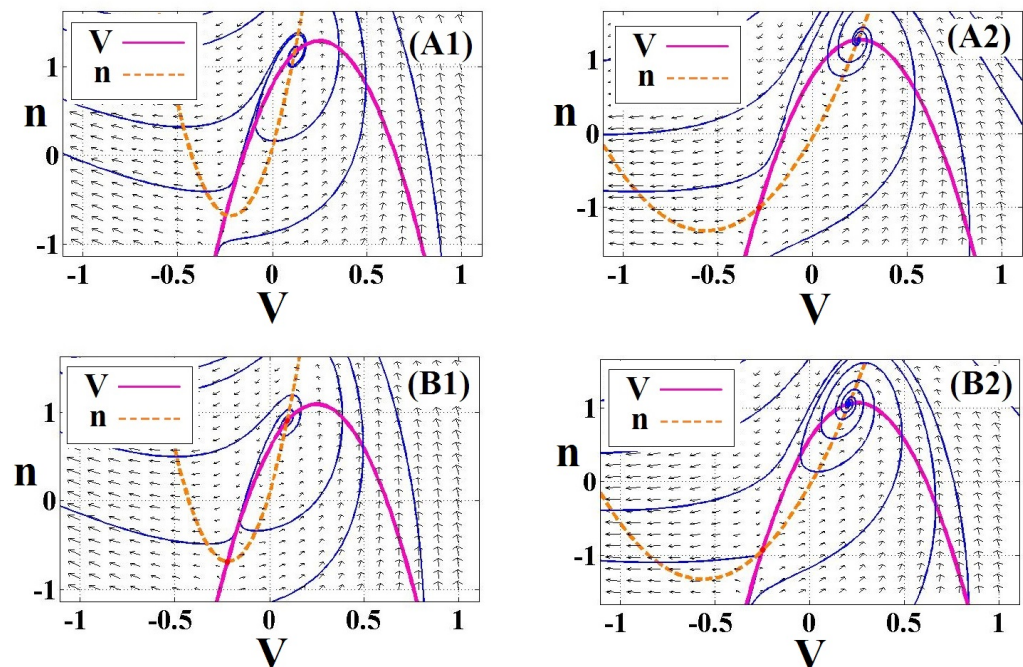
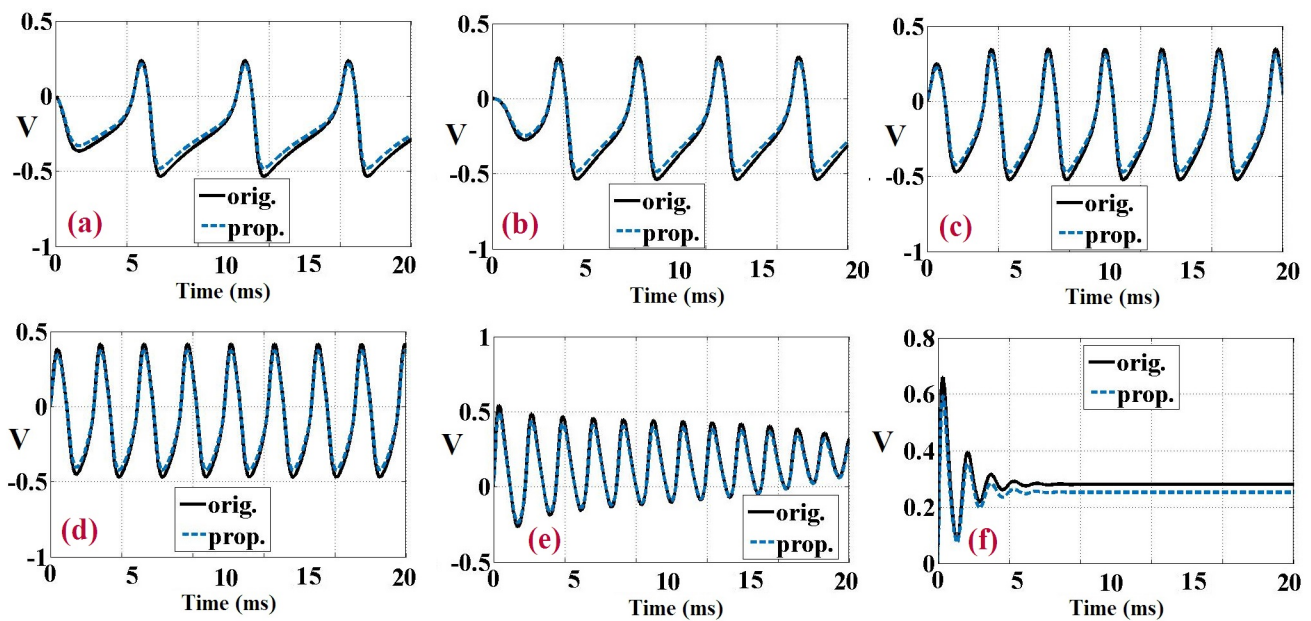


Figure 3. Dynamical behaviors for the original and proposed models. (A1,A2): Dynamics for the Class I and Class II patterns in the original model. (B1,B2): Dynamics for the Class I and Class II patterns in the proposed model. In these cases,  $n$  is the slow variable and  $V$  is the membrane potential. The equilibrium points of two original and proposed models are the same.

#### 4.2. Time Domain

To validate the proposed neuron model in case of timing accuracy and spiking patterns, the time domain must be considered. In this approach, based on different stimulus currents, the spiking patterns between original and proposed DSSN models are compared. As can be seen in Figure 4, spiking patterns of the proposed neuron model share a high degree of similarity with the original model. In addition, the error calculations are in a low state, which are computed in the next step.



**Figure 4.** Comparison between spiking patterns of two models (original and proposed). (a–f): Spiking patterns for considering the stimulus currents as:  $I_{Stimulus=0.1}$ ,  $I_{Stimulus=0.2}$ ,  $I_{Stimulus=0.5}$ ,  $I_{Stimulus=1}$ ,  $I_{Stimulus=2}$ , and  $I_{Stimulus=3}$ .

As can be seen in Figure 4, in some region of the spiking patterns, there are differences (errors) between the original and proposed DSSN models. Indeed, it is attempted to reduce this error to a near-zero value. A different method is available to calculate the error values between the original and proposed models. Some of these methods are focused on the absolute differences between two signals. In addition, some methods are emphasized on the square of root mean values. In this paper, these two basic error methods are applied for validating that the proposed model is in the low-error calculation compared with the original main model. These two methods are formulated as follows:

$$RMSE(V_{Prop.}, V_{Orig.}) = \sqrt{\frac{\sum_{i=1}^n (V_{Prop.} - V_{Orig.})^2}{n}} \tag{17}$$

$$MAE = \frac{1}{n} \sum_{i=1}^n |V_{Prop.} - V_{Orig.}| \tag{18}$$

Moreover, as can be seen in Figure 5, the error level is based on the differences between the original and proposed functions. Indeed, when this difference is accrued, the spiking patterns between the original and proposed models may have differences. These differences in our proposed models have been optimized, so the modified model regenerates the same behaviors of spike-based behavior of the original model to a high degree of similarity and low-error computations. As it is shown in Table 4, the error levels are calculated.

**Table 4.** Error Calculations of the Proposed Model.

$I_{Stimulus}$	RMSE (Class I)	MAE (Class I)	RMSE (Class II)	MAE (Class II)
0.1	0.05	0.02	0.067	0.022
0.2	0.08	0.01	0.1	0.018
0.5	0.09	0.034	0.095	0.04
1	0.1	0.028	0.15	0.039
2	0.075	0.014	0.035	0.012
3	0.11	0.08	0.16	0.06



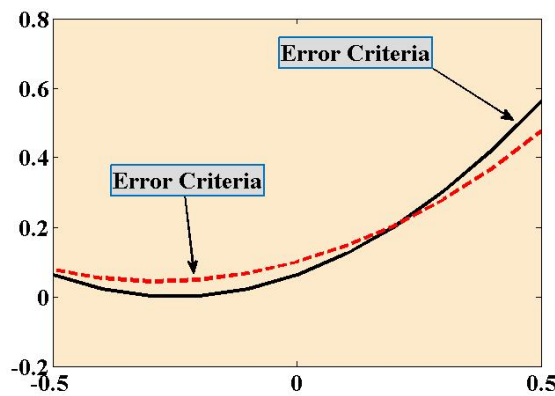


Figure 5. Error level between the original (black line) and proposed (dotted line) functions.

### 5. Synaptic Coupling

A synapse is a connection gap that can transfer data from a presynaptic neuron to a postsynaptic neuron. Synaptic coupling is a significant issue in the case of memory and learning. For describing the coupling behavior of two connected neurons, the synaptic coupling system can be evaluated [93,94]. In this approach, a terminal can be considered that incorporates a presynaptic neuron and a postsynaptic neuron. This synapse model can be given by the following equation:

$$\begin{cases} \tau_s \frac{dZ}{dt} = [1 + \tanh(S_s(V_{presynaptic} - h_s))](1 - Z) - \frac{Z}{d_s} \\ I_{Synapse} = k_s(Z - Z_0) \end{cases} \quad (19)$$

In the above equation, the parameter  $Z$  is the synapse factor. Moreover, the synaptic parameters are given by the following:

- $\tau_s$  : Time delay (s);
- $S_s$  : Responsible for the activation and relaxation of  $Z$ ;
- $d_s$  : Relaxing the parameter  $Z$ ;
- $h_s$  : Threshold parameter for the activation of  $Z$ ;
- $k_s$  : Conductivity parameter;
- $Z_0$  : Reference level of  $Z$  .

When the presynaptic neuron ( $V_{presynaptic}$ ) reaches its critical value (threshold voltage,  $h_s$ ), the signal transmission of connected neurons is computed. Moreover, the synapse stimulus,  $I_{synapse}$ , triggers the postsynaptic neuron. Table 5 shows the synapse parameters.

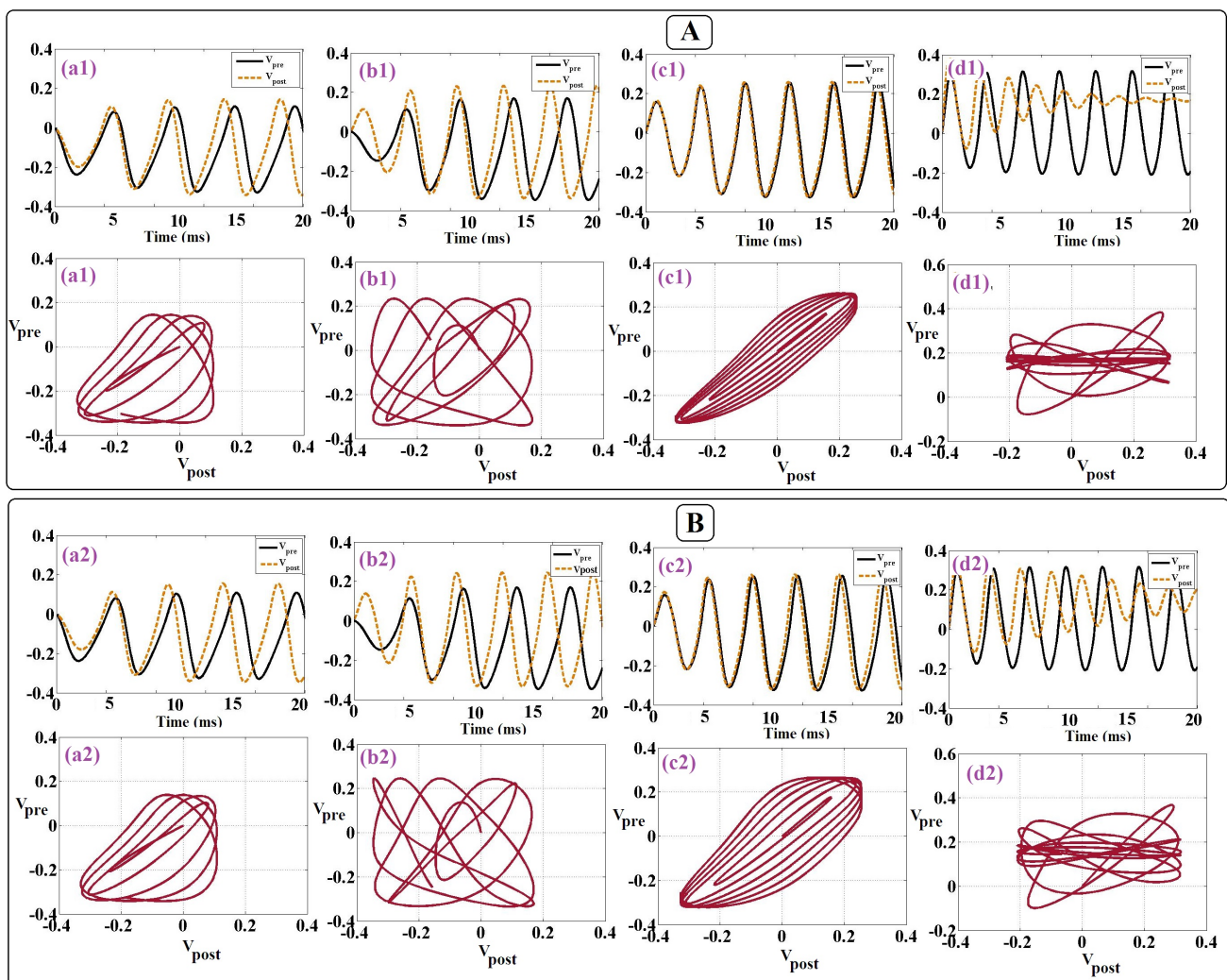
Table 5. Synapse Parameters.

$\tau_s = 10$	$S_s = 1$	$d_s = 3$	$h_s = -70$	$k_s = 10$	$Z_0 = 0$
---------------	-----------	-----------	-------------	------------	-----------

The synchronization effects of the coupled neurons are significant for the processing of biological signals and play significant roles in the elucidation of diseases, such as Parkinson’s disease, essential tremor, and epilepsy [95]. Consequently, by the appropriate selection of input stimulus and synaptic conductance coefficient, the synchronization effects can be controlled. This coupled proposed DSSN model is specified as follows:

$$\left\{ \begin{aligned}
 \frac{dV_{pre}}{dt} &= \frac{\phi}{\tau} (F(V_{pre}) - n_{pre} + I_0 + I_{Stimulus}) \\
 \frac{dn_{pre}}{dt} &= \frac{1}{\tau} (G(V_{pre}) - n_{pre}) \\
 \tau_s \frac{dZ}{dt} &= [1 + \tanh(S_s(V_{pre} - h_s))](1 - Z) - \frac{Z}{d_s} \\
 I_{synapse} &= k_s(Z - Z_0) \\
 \frac{dV_{post}}{dt} &= \frac{\phi}{\tau} (F(V_{post}) - n_{post} + I_0 + I_{synapse}) \\
 \frac{dn_{post}}{dt} &= \frac{1}{\tau} (G(V_{post}) - n_{post})
 \end{aligned} \right. \tag{20}$$

Consequently, by different stimulus currents, different states of the synchronization between presynaptic and postsynaptic neurons in the proposed and original models are evaluated. These states are depicted in Figure 6.



**Figure 6.** Time domain and dynamical portrait for two coupled DSSN models: (A) Original DSSN-coupled models that correspond to (a<sub>1</sub>–d<sub>1</sub>); (B) Proposed DSSN-coupled models by (a<sub>2</sub>–d<sub>2</sub>). These patterns are evoked by different stimulus as:  $I_{Stimulus} = 0.1$ ,  $I_{Stimulus} = 0.2$ ,  $I_{Stimulus} = 0.5$ , and  $I_{Stimulus} = 1$ , respectively.

### 6. Overall Hardware Implementation

This section presents a comprehensive digital architecture based on the proposed neuron model using FPGA board hardware. For implementing a mathematical neuron equation on FPGA hardware, different issues must be taken into account. In our paper, since the final goal is the realization of a compact hardware with low-cost and high-speed attributes, the first step is determining the bit-width, which must be in optimized state. On the other hand, based on the proposed equations, the scheduling diagrams are created to consider the final routes in the hardware implementation. In this state, the pipeline approach can be applied to accelerate the output signals execution. In our architecture, all of functions and terms of the model are realized without any using multiplier operations. This causes the final proposed hardware to have a high-frequency and low-resources area in comparison with the original one. After this state, we can use the Hardware Description Language (HDL) to create the proposed digital code. In this way, different approaches are used to obtain a low-cost implementation in FPGA level. Consequently, using the proposed method, we have an efficient hardware that can be used as high-speed digital equipment in spiking neural networks area.

#### 6.1. Scheduling Diagrams

In this part, based on the proposed model (equations), the final scheduling diagrams are created. In this approach, we have two basic variables ( $V$  and  $n$ ) which are scheduled as two main hardware routes. For considering the proposed model in hardware form, it is essential that the hyperbolic terms of this model is reformulated (as a discretized form) as below:

$$Func(V[i]) = 0.6 \left[ \frac{2^{0.65V[i]} - 2^{-0.65V[i]}}{2} \right] + 0.6 \left[ \frac{2^{0.65V[i]} + 2^{-0.65V[i]}}{2} \right] - 0.5 \quad (21)$$

For implementing this function, the power2-based approximation can be used [68]. Generating the exponential functions (EXP. Unit) with powers of 2, is the key idea of this approach, which is realized by a logic shift. Replacing multipliers with logic shift operations leads to a significant low-cost hardware realization. As a result, in this approach, the hyperbolic terms will be achieved. As depicted in Figure 7, this hyperbolic function can be created.

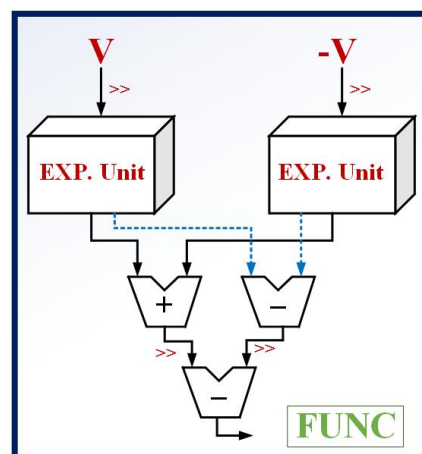


Figure 7. Realization of the proposed  $FUNC(V)$  function.

In the next step, using this  $FUNC(V)$  hardware, the hardware of the internal functions ( $F(V)$ ,  $G(V)$ ) are realized, based on the following discretized equations:

$$F(V[i]) = \begin{cases} a_n(Func(V[i])) - c_n & ; V[i] < 0 \\ -a_p(Func(V[i]) - 4V[i]b_n) + c_p & ; V[i] > 0 \end{cases} \quad (22)$$

$$G(V[i]) = \begin{cases} k_n(\text{Func}(V[i])) + q_n & ; V[i] < r \\ k_p(\text{Func}(V[i])) + q_p & ; V[i] > r \end{cases} \tag{23}$$

These two internal terms are realized, as can be depicted in Figure 8.

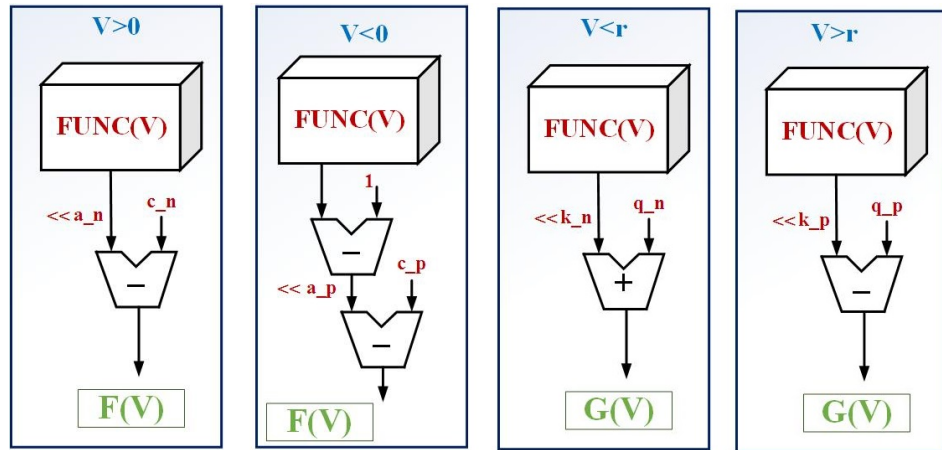


Figure 8. Realization of the proposed  $F(V)$  and  $G(V)$  functions.

Consequently, using the above internal functions, the scheduling diagrams of the proposed model can be designed based on the following discretized equations:

$$V[i + 1] = dt * \frac{\phi}{\tau} (F(V[i]) - n[i] + I_0 + I_{Stimulus}) + V[i] \tag{24}$$

$$n[i + 1] = dt * \frac{1}{\tau} (G(V[i]) - n[i]) + n[i] \tag{25}$$

The scheduling diagrams of the proposed equations are depicted in Figure 9.

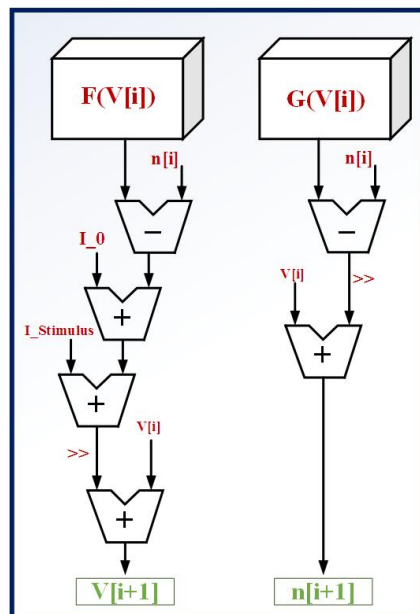


Figure 9. Scheduling diagrams for realizing the basic variables,  $V$  and  $n$ .

As can be seen from the scheduling diagrams, the proposed neuron model can be implemented as a digital system in a multiplierless state. All of the proposed terms and equations of the implemented model have been realized based on the primary blocks such as ADDs, SUBs, and digital SHIFTs. In other words, using the proposed method, the final digital costs will be significantly reduced. This approach causes a speed-up (by increasing

the system frequency) in the digital hardware that can be implemented on FPGA platforms. One of the important issues in the neural networks is the large-scale realization of the brain network. Indeed, if the maximum number of digitally implemented neurons is increased, we have a real neuromorphic hardware that is capable of reproducing brain behaviors. Consequently, the proposed model can be considered as a low-cost digital system that is used in the brain network.

### 6.2. Bit-Width Definition

In digital implementation, it is essential that the proposed model bit-width is described in detail for reducing the final hardware costs. As a first step, based on all parameters and variables of the proposed model, the number of integers and fraction parts must be calculated. In this way, for the proposed DSSN model, the maximum and minimum values are 16 and  $-1.3177$ , respectively. These values require the bit number of 4 and 3 for the integer and the fraction parts, respectively. Thus, in the first state, the number of 7 can be required. Moreover, based on the scheduling diagrams of the proposed DSSN neuron model (Figure 9), in the generating paths of the output signals ( $V$  and  $n$ ), the signals may be shifted to the right and left. In this condition, the bit-width is significantly varied. Based on the final calculations, by shifting the signals to the right in the semi-final steps of the basic variables, the number of 8 is added to the fraction part of the bit-width. Moreover, one bit must be calculated for the sign bit of the proposed system. Consequently, the bit-width of the final system is calculated as 16. In this calculation, the number of 4 for the integer part, the number of 11 for the fraction section, and 1 bit for sign bit are required.

### 6.3. Architecture Design

After presenting the scheduling diagrams of the proposed model, it is required that the proposed architecture of the digital design is considered. The overall architecture of the proposed model is depicted in Figure 10.

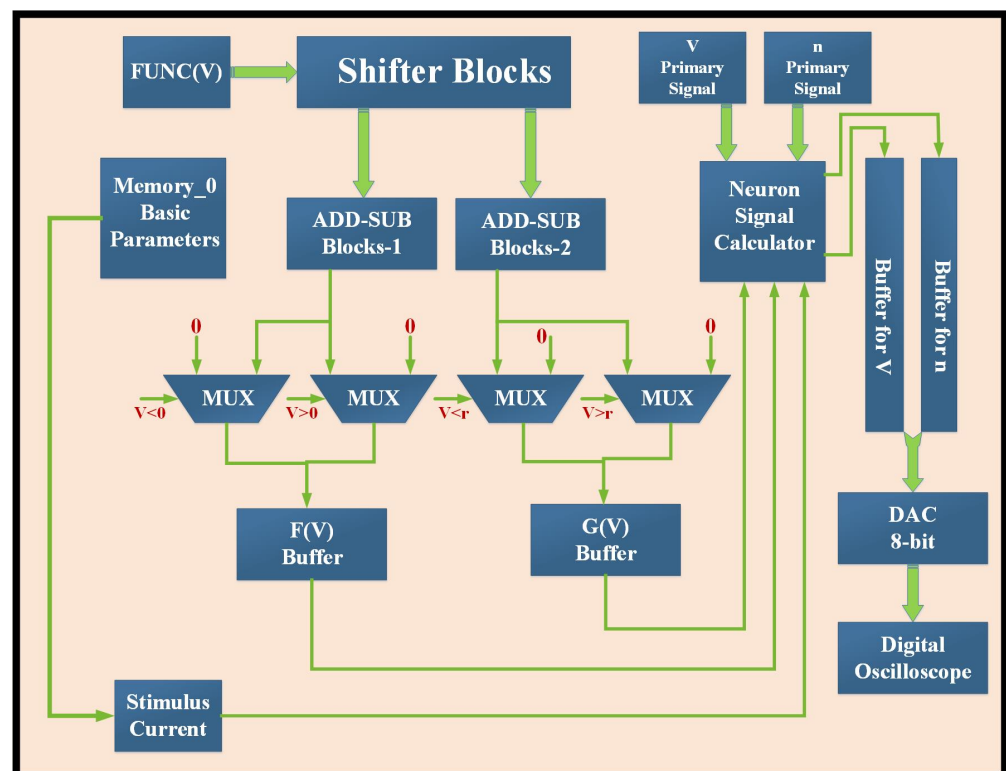


Figure 10. The overall structure of the proposed architecture based on the DSSN equations and scheduling diagrams.

As can be seen in this figure, the model parameters are saved in the *Memory<sub>0</sub>* block (parameters that are presented in Tables 1 and 2). At first step, the  $FUNC(V)$  term is realized based on the proportional scheduling diagram. After creating this basic function, some *ShifterBlocks* (based on the Equations (7) and (8)) are applied for generating the two basic functions,  $F(V)$  and  $G(V)$ . Then, by considering some *Multiplexer Blocks*, the final terms can be realized. These final terms and also primary signals of the basic variables ( $V$  and  $n$ ) are applied to the *Neuron Signal Calculator*. This core unit is responsible for reproducing the final voltage signals based on the DSSN neuron model. The neuron calculator unit is based on the scheduling diagram that is presented in Figure 9. Finally, the neuron signals are transferred to two buffers (*Buffer V* and *Buffer n*). Consequently, the final signals are applied to an 8-bit DAC (Digital to Analog Converter) and can be showed on the digital oscilloscope.

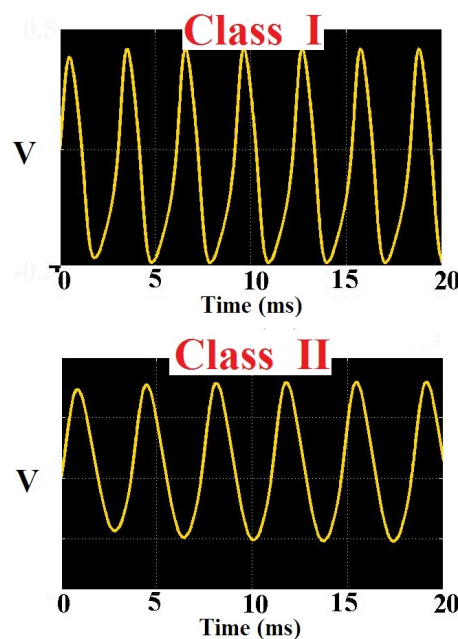
## 7. Production Results

The basic units of the hardware implementation are: scheduling diagrams of the basic variables, the overall architecture, and the bit-width definition. Indeed, after bit-width definition, the scheduling diagrams of the basic variables ( $V$  and  $n$ ) are evaluated. In this state, all aspects have been considered to achieve an HDL digital code. On the other hand, the overall architecture is presented to show the controlling sequence of the digital implementation.

To validate the proposed DSSN model and compare this model with other implementations, it is essential that a digital hardware is selected for realizing these models on digital platforms. In this paper, the original and proposed neuron models are implemented on Xilinx Spartan-3 FPGA Board (Model: XC3S50-TQ144 Package) for validating the proposed method. On the other hand, the proposed neuron model is compared by the DSSN model that is implemented in other similar papers [96]. Using the pipelining method, the number of 250 connected neurons can be implemented on this FPGA platform by resource utilization that is presented in Table 6. Two basic factors must be emphasized in this issue: first is the maximum frequency of the digital design and second is the overall saving in FPGA resources (in case of maximum number of implemented neurons on a unique FPGA core). As can be seen from Table 6, these two parameters are in the better form in comparison to the main DSSN model and also in comparison to the model presented in [96]. As previously mentioned, since in the proposed DSSN model, all of nonlinear parts (such as multipliers and quadratic functions) are replaced by digital SHIFTs, ADDs, and SUBs, the final frequency of the digital system will be increased, significantly. Moreover, by removing the multiplier operations in the proposed model, the overhead costs will be reduced compared to other similar models. As a result, one of the basic parameters in the realization of neural networks is the large-scale implementation. In this approach, the overall saving in the FPGA resources is an essential issue. In this paper, the overall saving in FPGA resources is higher than the original and other paper model [96]. On the other hand, using an FPGA board, the maximum number of implemented proposed neurons is higher than other models because in the Spartan-3 board that we used, the number of resources are less than the Spartan-6 FPGA board that is used in [96]. Consequently, the proposed model is in the better state in the case of large numbers of implemented neurons compared to other methods. As a result, the final FPGA-based output signals can be achieved as depicted in Figure 11. As it is illustrated in this figure, the proposed signals (implemented on FPGA board) are in the high similarity state in comparison with the original output voltage signals.

**Table 6.** FPGA Utilization Results for the Different DSSN Models.

Resources	Proposed DSSN (Spartan-3)	Original DSSN (Spartan-3)	J. Li [96] (Spartan-6)
Number of Slices	158 (21%)	610 (82%)	14,198 (26%)
Number of Slice Flip Flops	445 (29%)	1150 (75%)	NA
Number of 4 input LUTs	953 (62%)	1050 (69%)	18,556 (68%)
Number of bonded IOBs	27 (5%)	34 (6%)	NA
Number of GCLKs	1 (6%)	1 (6%)	NA
DSP	NA	NA	48 (82%)
Block RAMs	NA	NA	73 (63%)
Max Speed	168 MHz	63 MHz	NA



**Figure 11.** Digital oscilloscope for the proposed output signals (class I and class II in terms of  $I_{stimulus} = 1$ ). Two basic spiking patterns (Class I and Class II) are presented for the voltage variable.

**8. Discussion**

Digital implementation of different parts of the central nervous system is an attractive research field for achieving a real and practical system. In this area, the basic elements of this nervous system are: neurons, synapses, and glia with large number populations and a complex real network. Thus, to have a real system, it is necessary that the large number of these neuronal cells are realized and that the complexity of their connections are also considered. As a result, the basic limitation of this issue is the large-scale digital implementation of these networks and their complex connections. On the other hand, since the hardware platforms such as FPGA have limitations (in case of internal resources), to achieve a real and large-scale design, a large number of FPGA boards must be used, which can be a vital limitations in this field. Consequently, one of the topics that can be discussed, studied, and implemented in the continuation of this type of issue is the implementation of large networks of these neurons so that we can come closer to the real brain networks. With such real systems, we can study some of the underlying brain diseases and perhaps find solutions to treat them.

**9. Conclusions**

The simulation and implementation of neuronal networks are the attractive research area and this requires knowledge of the central nervous system and its components. Thus, modeling the neuronal behaviors must be very significant in case of using in the neuromorphic field. The realization of these models in low-cost and high-speed form is an essential

issue targeting large-scale neuromorphic networks. Different approaches can be applied for implementing these neuron models, but the target approach must cover all aspects of an efficient digital design (without any nonlinear and high-cost terms implementation such as multipliers, dividers, exponential units, quadratic terms, etc.). Consequently, in this paper, a hyperbolic-based of the DSSN neuron model is presented in case of power-2 functions without any multiplications. The proposed architecture can reproduce two basic classes of spiking signals in a good similarity and efficiency. This approach causes reducing in error calculation and increasing performances of the system in case of decreasing the required resources on FPGA platform. Since the nonlinear parts of the DSSN neural modeling have been removed, we have a multiplierless digital implementation. The proposed designed system is in the high-frequency state and has an observable cost reduction in FPGA resources compared with similar implemented neuron models. For validating and confirming the proposed approach design, Spartan-3 FPGA board can be used and considered. In this way, hardware results show that this new model is capable for mimicking the same behaviors of the original neuronal modeling. The new proposed hardware can follow the original model in case of higher frequency and also low-cost realization condition. The results of implementation show the better state in overall saving in FPGA and also higher frequency of the proposed model about 168 MHz, which is significantly higher than the original model, 63 MHz.

**Author Contributions:** Methodology, M.B. and E.E.-Z.; software, O.T. and M.T.Y.; data curation, O.T.; writing—original draft preparation, M.T.Y. and M.A.; writing—review and editing, E.E.-Z. and M.B.; investigation, M.A. and M.B.; visualization, M.T.Y. and M.A.; supervision, E.N.; funding acquisition, M.B. All authors have read and agreed to the published version of the manuscript.

**Funding:** The authors extend their appreciation to the Deputyship for Research and Innovation, Ministry of Education in Saudi Arabia, for funding this research work through the project number (IFPHI-323-135-2020) and King Abdulaziz University, DSR, Jeddah, Saudi Arabia.

**Institutional Review Board Statement:** Not applicable.

**Informed Consent Statement:** Not applicable.

**Data Availability Statement:** Data are contained within the article.

**Acknowledgments:** We acknowledge support of the Open Access Publication Fund of the Thueringer Universitaetsund Landesbibliothek Jena.

**Conflicts of Interest:** The authors declare no conflict of interest.

## References

1. Roshani, G.H.; Feghhi, S.A.H.; Mahmoudi-Aznavah, A.; Nazemi, E.; Adineh-Vand, A. Precise volume fraction prediction in oil-water-gas multiphase flows by means of gamma-ray attenuation and artificial neural networks using one detector. *Measurement* **2014**, *51*, 34–41. [[CrossRef](#)]
2. Nazemi, E.; Feghhi, S.; Roshani, G.; Setayeshi, S.A.; Peyvandi, R.G. A radiation-based hydrocarbon two-phase flow meter for estimating of phase fraction independent of liquid phase density in stratified regime. *Flow Meas. Instrum.* **2015**, *46*, 25–32. [[CrossRef](#)]
3. Roshani, G.H.; Nazemi, E.; Feghhi, S.A.; Setayeshi, S. Flow regime identification and void fraction prediction in two-phase flows based on gamma ray attenuation. *Measurement* **2015**, *62*, 25–32. [[CrossRef](#)]
4. Roshani, G.H.; Nazemi, E.; Feghhi, S.A.H. Investigation of using  $^{60}\text{Co}$  source and one detector for determining the flow regime and void fraction in gas-liquid two-phase flows. *Flow Meas. Instrum.* **2016**, *50*, 73–79. [[CrossRef](#)]
5. Nazemi, E.; Feghhi, S.; Roshani, G.; Peyvandi, R.G.; Setayeshi, S. Precise void fraction measurement in two-phase flows independent of the flow regime using gamma-ray attenuation. *Nucl. Eng. Technol.* **2016**, *48*, 64–71. [[CrossRef](#)]
6. Roshani, G.H.; Nazemi, E.; Roshani, M.M. Flow regime independent volume fraction estimation in three-phase flows using dual-energy broad beam technique and artificial neural network. *Neural Comput. Appl.* **2016**, *28*, 1265–1274. [[CrossRef](#)]
7. Nazemi, E.; Roshani, G.H.; Feghhi, S.A.H.; Setayeshi, S.; Eftekhari Zadeh, E.; Fatehi, A. Optimization of a method for identifying the flow regime and measuring void fraction in a broad beam gamma-ray attenuation technique. *Int. J. Hydrogen Energy* **2016**, *41*, 7438–7444. [[CrossRef](#)]



8. Alanazi, A.K.; Alizadeh, S.M.; Nurgalieva, K.S.; Guerrero, J.W.G.; Abo-Dief, H.M.; Eftekhari-Zadeh, E.; Narozhnyy, I.M. Optimization of x-ray tube voltage to improve the precision of two phase flow meters used in petroleum industry. *Sustainability* **2021**, *13*, 3622. [[CrossRef](#)]
9. Roshani, G.; Nazemi, E.; Roshani, M. Usage of two transmitted detectors with optimized orientation in order to three phase flow metering. *Measurement* **2017**, *100*, 122–130. [[CrossRef](#)]
10. Roshani, G.; Nazemi, E. Intelligent densitometry of petroleum products in stratified regime of two phase flows using gamma ray and neural network. *Flow Meas. Instrum.* **2017**, *58*, 6–11. [[CrossRef](#)]
11. Roshani, G.; Nazemi, E.; Roshani, M. Intelligent recognition of gas-oil-water three-phase flow regime and determination of volume fraction using radial basis function. *Flow Meas. Instrum.* **2017**, *54*, 39–45. [[CrossRef](#)]
12. Roshani, G.; Nazemi, E.; Roshani, M. Identification of flow regime and estimation of volume fraction independent of liquid phase density in gas-liquid two-phase flow. *Prog. Nucl. Energy* **2017**, *98*, 29–37. [[CrossRef](#)]
13. Karami, A.; Roshani, G.H.; Nazemi, E.; Roshani, S. Enhancing the performance of a dual-energy gamma ray based three-phase flow meter with the help of grey wolf optimization algorithm. *Flow Meas. Instrum.* **2018**, *64*, 164–172. [[CrossRef](#)]
14. Roshani, G.H.; Roshani, S.; Nazemi, E.; Roshani, S. Online measuring density of oil products in annular regime of gas-liquid two phase flows. *Measurement* **2018**, *129*, 296–301. [[CrossRef](#)]
15. Roshani, G.; Hanus, R.; Khazaei, A.; Zych, M.; Nazemi, E.; Mosorov, V. Density and velocity determination for single-phase flow based on radiotracer technique and neural networks. *Flow Meas. Instrum.* **2018**, *61*, 9–14. [[CrossRef](#)]
16. Khaibullina, K.S.; Sagirova, L.R.; Sandyga, M.S. Substantiation and selection of an inhibitor for preventing the formation of asphalt-resin-paraffin deposits. *Period. Tche Quim.* **2020**, *17*, 541–551. [[CrossRef](#)]
17. Karami, A.; Roshani, G.H.; Khazaei, A.; Nazemi, E.; Fallahi, M. Investigation of different sources in order to optimize the nuclear metering system of gas-oil-water annular flows. *Neural Comput. Appl.* **2020**, *32*, 3619–3631. [[CrossRef](#)]
18. Roshani, M.; Sattari, M.A.; Muhammad Ali, P.J.; Roshani, G.H.; Nazemi, B.; Corniani, E.; Nazemi, E. Application of GMDH neural network technique to improve measuring precision of a simplified photon attenuation based two-phase flowmeter. *Flow Meas. Instrum.* **2020**, *75*, 101804. [[CrossRef](#)]
19. Pirasteh, A.; Roshani, S.; Roshani, S. A modified class-F power amplifier with miniaturized harmonic control circuit. *AEU-Int. J. Electron. Commun.* **2018**, *97*, 202–209. [[CrossRef](#)]
20. Roshani, S.; Roshani, S. Design of a very compact and sharp bandpass diplexer with bended lines for GSM and LTE applications. *AEU-Int. J. Electron. Commun.* **2019**, *99*, 354–360. [[CrossRef](#)]
21. Pirasteh, A.; Roshani, S.; Roshani, S. Compact microstrip lowpass filter with ultrasharp response using a square-loaded modified T-shaped resonator. *Turk. J. Electr. Eng. Comput. Sci.* **2018**, *26*, 1736–1746. [[CrossRef](#)]
22. Jamshidi, M.B.; Roshani, S.; Talla, J.; Roshani, S.; Peroutka, Z. Size reduction and performance improvement of a microstrip Wilkinson power divider using a hybrid design technique. *Sci. Rep.* **2021**, *11*, 7773. [[CrossRef](#)] [[PubMed](#)]
23. Roshani, S.; Roshani, S. Design of a high efficiency class-F power amplifier with large signal and small signal measurements. *Measurement* **2020**, *149*, 106991. [[CrossRef](#)]
24. Roshani, S.; Roshani, S.; Zarinitabar, A. A modified Wilkinson power divider with ultra harmonic suppression using open stubs and lowpass filters. *Analog. Integr. Circuits Signal Process.* **2019**, *98*, 395–399. [[CrossRef](#)]
25. Jamshidi, M.; Siahkamari, H.; Roshani, S.; Roshani, S. A compact Gysel power divider design using U-shaped and T-shaped resonators with harmonics suppression. *Electromagnetics* **2019**, *39*, 491–504. [[CrossRef](#)]
26. Roshani, S.; Jamshidi, M.B.; Mohebi, F.; Roshani, S. Design and modeling of a compact power divider with squared resonators using artificial intelligence. *Wirel. Pers. Commun.* **2021**, *117*, 2085–2096. [[CrossRef](#)]
27. Chuang, M.-L. Dual-Band Impedance Transformer Using Two-Section Shunt Stubs. *IEEE Trans. Microw. Theory Tech.* **2010**, *58*, 1257–1263. [[CrossRef](#)]
28. Roshani, S.; Roshani, S. A compact coupler design using meandered line compact microstrip resonant cell (MLCMRC) and bended lines. *Wirel. Netw.* **2021**, *27*, 677–684. [[CrossRef](#)]
29. Lalbakhsh, A.; Mohamadpour, G.; Roshani, S.; Ami, M.; Roshani, S.; Sayem, A.S.; Alibakhshikenari, M.; Koziel, S. Design of a compact planar transmission line for miniaturized rat-race coupler with harmonics suppression. *IEEE Access* **2021**, *9*, 129207–129217. [[CrossRef](#)]
30. Lalbakhsh, A.; Afzal, M.U.; Esselle, K.P.; Manda, K. All-Metal Wideband Frequency-Selective Surface Bandpass Filter for TE and TM polarizations. *IEEE Trans. Antennas Propag.* **2022**. [[CrossRef](#)]
31. Lalbakhsh, A.; Afzal, M.U.; Hayat, T.; Esselle, K.P.; Manda, K. All-metal wideband metasurface for near-field transformation of medium-to-high gain electromagnetic sources. *Sci. Rep.* **2021**, *11*, 9421. [[CrossRef](#)]
32. Lalbakhsh, A.; Alizadeh, S.M.; Ghaderi, A.; Golestanifar, A.; Mohamadzade, B.; Jamshidi, M.B.; Mandal, K.; Mohyuddin, W. A Design of a Dual-Band Bandpass Filter Based on Modal Analysis for Modern Communication Systems. *Electronics* **2020**, *9*, 1770. [[CrossRef](#)]
33. Lalbakhsh, A.; Jamshidi, M.B.; Siahkamari, H.; Ghaderi, A.; Golestanifar, A.; Linhart, R.; Talla, J.; Simorangkir, R.B.; Mandal, K. A Compact Lowpass Filter for Satellite Communication Systems Based on Transfer Function Analysis. *AEU-Int. J. Electron. Commun.* **2020**, *124*, 153318. [[CrossRef](#)]

34. Lalbakhsh, A.; Ghaderi, A.; Mohyuddin, W.; Simorangkir, R.B.V.B.; Bayat-Makou, N.; Ahmad, M.S.; Lee, G.H.; Kim, K.W. A Compact C-Band Bandpass Filter with an Adjustable Dual-Band Suitable for Satellite Communication Systems. *Electronics* **2020**, *9*, 1088. [[CrossRef](#)]
35. Alanazi, A.K.; Alizadeh, S.M.; Nurgalieva, K.S.; Nestic, S.; Grimaldo Guerrero, J.W.; Abo-Dief, H.M.; Eftekhari-Zadeh, E.; Nazemi, E.; Narozhnyy, I.M. Application of Neural Network and Time-Domain Feature Extraction Techniques for Determining Volumetric Percentages and the Type of Two Phase Flow Regimes Independent of Scale Layer Thickness. *Appl. Sci.* **2022**, *12*, 1336. [[CrossRef](#)]
36. Lalbakhsh, A.; Afzal, M.U.; Esselle, K. Simulation-driven particle swarm optimization of spatial phase shifters. In Proceedings of the 18th IEEE international Conference on Electromagnetics in Advanced Applications (ICEAA), Cairns, Australia, 19–23 September 2016; pp. 428–430. [[CrossRef](#)]
37. Lalbakhsh, A.; Afzal, M.U.; Esselle, K.P.; Smith, S.L. Low-Cost Non-Uniform Metallic Lattice for Rectifying Aperture Near-Field of Electromagnetic Bandgap Resonator Antennas. *IEEE Trans. Antennas Propag.* **2020**, *68*, 3328–3335. [[CrossRef](#)]
38. Paul, G.S.; Mandal, K.; Lalbakhsh, A. Single-layer ultra-wide stop-band frequency selective surface using interconnected square rings. *AEU-Int. J. Electron. Commun.* **2021**, *132*, 153630. [[CrossRef](#)]
39. Lalbakhsh, A.; Lotfi-Neyestanak, A.A.; Naser-Moghaddasi, M. Microstrip Hairpin Bandpass Filter Using Modified Minkowski Fractal for Suppression of Second Harmonic. *IEICE. Trans. Electron.* **2012**, *E95-C*, 378–381. [[CrossRef](#)]
40. Khaibullina, K.S.; Korobov, G.Y.; Lekomtsev, A.V. Development of an asphalt-resin-paraffin deposits inhibitor and substantiation of the technological parameters of its injection into the bottom-hole formation zone. *Period. Tche Quim.* **2020**, *17*, 769–781. [[CrossRef](#)]
41. Roshani, M.; Phan, G.; Faraj, R.H.; Phan, N.H.; Roshani, G.H.; Nazemi, B.; Corniani, E.; Nazemi, E. Proposing a gamma radiation based intelligent system for simultaneous analyzing and detecting type and amount of petroleum by-products. *Neural Eng. Technol.* **2021**, *53*, 1277–1283. [[CrossRef](#)]
42. Roshani, M.; Phan, G.T.; Ali, P.J.M.; Roshani, G.H.; Hanus, R.; Duong, T.; Corniani, E.; Nazemi, E.; Kalmoun, E.M. Evaluation of flow pattern recognition and void fraction measurement in two phase flow independent of oil pipeline's scale layer thickness. *Alex. Eng. J.* **2021**, *60*, 1955–1966. [[CrossRef](#)]
43. Roshani, M.; Phan, G.; Roshani, G.H.; Hanus, R.; Nazemi, B.; Corniani, E.; Nazemi, E. Combination of X-ray tube and GMDH neural network as a nondestructive and potential technique for measuring characteristics of gas-oil-water three phase flows. *Measurement* **2021**, *168*, 108427. [[CrossRef](#)]
44. Tikhomirova, E.A.; Sagirova, L.R.; Khaibullina, K.S. A review on methods of oil saturation modelling using IRAP RMS. In Proceedings of the IOP Conference Series: Earth and Environmental Science, Saint-Petersburg, Russia, 24–27 April 2019; Volume 378. [[CrossRef](#)]
45. Sattari, M.A.; Roshani, G.H.; Hanus, R.; Nazemi, E. Applicability of time-domain feature extraction methods and artificial intelligence in two-phase flow meters based on gamma-ray absorption technique. *Measurement* **2021**, *168*, 108474. [[CrossRef](#)]
46. Roshani, S.; Roshani, S. Two-Section Impedance Transformer Design and Modeling for Power Amplifier Applications. *Appl. Comput. Electromagn. Soc. J.* **2017**, *32*, 1042–1047.
47. Khaibullina, K. Technology to remove asphaltene, resin and paraffin deposits in wells using organic solvents. In Proceedings of the SPE Annual Technical Conference and Exhibition, Dubai, United Arab Emirates, 26–28 September 2016.
48. Lv, Z.; Guo, J.; Lv, H. Safety Poka Yoke in Zero-Defect Manufacturing Based on Digital Twins. *IEEE Trans. Ind. Inform.* **2022**. [[CrossRef](#)]
49. Liu, X.; Zhao, J.; Li, J.; Cao, B.; Lv, Z. Federated Neural Architecture Search for Medical Data Security. *IEEE Trans. Ind. Inform.* **2022**. [[CrossRef](#)]
50. Cao, B.; Zhao, J.; Liu, X.; Arabas, J.; Tanveer, M.; Singh, A.K.; Lv, Z. Multiobjective Evolution of the Explainable Fuzzy Rough Neural Network with Gene Expression Programming. *IEEE Trans. Fuzzy Syst.* **2022**. [[CrossRef](#)]
51. He, Z.-Y.; Abbes, A.; Jahanshahi, H.; Alotaibi, N.D.; Wang, Y. Fractional-order discrete-time SIR epidemic model with vaccination: Chaos and complexity. *Mathematics* **2022**, *10*, 165. [[CrossRef](#)]
52. Li, B.; Yang, J.; Yang, Y.; Li, C.; Zhang, Y. Sign Language/Gesture Recognition Based on Cumulative Distribution Density Features Using UWB Radar. *IEEE Trans. Instrum. Meas.* **2021**. [[CrossRef](#)]
53. Mi, C.; Chen, J.; Zhang, Z.; Huang, S.; Postolache, O. Visual Sensor Network Task Scheduling Algorithm at Automated Container Terminal. *IEEE Sens. J.* **2021**. [[CrossRef](#)]
54. Che, H.; Wang, J. A Two-Timescale Duplex Neurodynamic Approach to Mixed-Integer Optimization. *IEEE Trans. Neural Netw. Learn. Syst.* **2021**, *32*, 36–48. [[CrossRef](#)] [[PubMed](#)]
55. Zheng, W.; Liu, X.; Ni, X.; Yin, L.; Yang, B. Improving Visual Reasoning Through Semantic Representation. *IEEE Access* **2021**, *9*, 91476–91486. [[CrossRef](#)]
56. Zheng, W.; Liu, X.; Yin, L. Sentence Representation Method Based on Multi-Layer Semantic Network. *Appl. Sci.* **2021**, *11*, 1316. [[CrossRef](#)]
57. Tang, Y.; Liu, S.; Deng, Y.; Zhang, Y.; Yin, L.; Zheng, W. An improved method for soft tissue modeling. *Biomed. Signal Process. Control.* **2021**, *65*, 102367. [[CrossRef](#)]
58. Ghimire, P. Digitalization of Indigenous Knowledge in Nepal—Review Article. *Acta Inform. Malays.* **2021**, *5*, 42–47.
59. Wang, H.; Zhao, J. The Research in Digital Slope Information Technology: Evidences from Coastal Region of China. *J. Coast. Res.* **2020**, *103*, 798–801. [[CrossRef](#)]

60. Meng, F.; Pang, A.; Dong, X.; Han, C.; Sha, X. H Optimal Performance Design of an Unstable Plant under Bode Integral Constraint. *Complexity* **2018**, *2018*, 4942906. [[CrossRef](#)]
61. Meng, F.; Wang, D.; Yang, P.; Xie, G. Application of Sum of Squares Method in Nonlinear H Control for Satellite Attitude Maneuvers. *Complexity* **2019**, *2019*, 5124108. [[CrossRef](#)]
62. Hajiseyedazizi, S.N.; Samei, M.E.; Alzabut, J.; Chu, Y.-M. On multi-step methods for singular fractional q-integro-differential equations. *Open Math.* **2021**, *19*, 1–28. [[CrossRef](#)]
63. Jin, F.; Qian, Z.-S.; Chu, Y.-M.; ur Rahman, M. On nonlinear evolution model for drinking behavior under Caputo-Fabrizio derivative. *J. Appl. Anal. Comput.* **2022**. [[CrossRef](#)]
64. Rashid, S.; Abouelmagd, E.I.; Khalid, A.; Farooq, F.B.; Chu, Y.-M. Some recent developments on dynamical discrete fractional type inequalities in the frame of nonsingular and nonlocal kernels. *Fractals* **2022**, *30*, 2240110. [[CrossRef](#)]
65. Wang, F.-Z.; Khan, M.N.; Ahmad, I.; Ahmad, H.; Abu-Zinadah, H.; Chu, Y.-M. Numerical solution of traveling waves in chemical kinetics: Time-fractional fishers equations. *Fractals* **2022**, *30*, 22400051. [[CrossRef](#)]
66. Murtafiah, B.; Putro, N.H. Digital Literacy in The English Curriculum: Models of Learning Activities. *Acta Inform. Malays.* **2019**, *3*, 10–13. [[CrossRef](#)]
67. Haghiri, S.; Ahmadi, A.; Saif, M. VLSI implementable neuron-astrocyte control mechanism. *Neurocomputing* **2016**, *214*, 280–296. [[CrossRef](#)]
68. Gomar, S.; Ahmadi, A. Digital multiplierless implementation of biological adaptive-exponential neuron model. *IEEE Trans. Circuits Syst. I* **2013**, *61*, 1206–1219. [[CrossRef](#)]
69. Yu, T.; Sejnowski, T.J.; Cauwenberghs, G. Biophysical Neural Spiking, Bursting, and Excitability Dynamics in Reconfigurable Analog VLSI. *IEEE Trans. Biomed. Circuits Syst.* **2011**, *5*, 420–429. [[CrossRef](#)]
70. Heidarpur, M.; Ahmadi, A.; Ahmadi, M.; Azghadi, M.R. CORDIC-SNN: On-FPGA STDP Learning With Izhikevich Neurons. *IEEE Trans. Circuits Syst.-I* **2019**, *66*, 2651–2661. [[CrossRef](#)]
71. Indiveri, G.; Chicca, E.; Douglas, R. A VLSI array of low-power spiking neurons and bistable synapses with spike-timing dependent plasticity. *IEEE Trans. Neural Netw.* **2006**, *13*, 211–221. [[CrossRef](#)]
72. Rinzel, J.; Ermentrout, G.B. Analysis of Neural Excitability and Oscillations. *Methods Neuronal Model. Synapses Netw.* **1989**, 135–169.
73. Araque, A.; Parpura, V.; Sanzgiri, R.P.; Haydon, P.G. Tripartite synapses: Glia, the unacknowledged partner. *Trends Neurosci.* **1999**, *22*, 208–215. [[CrossRef](#)]
74. Volman, V.; Ben-Jacob, E.; Levine, H. The astrocyte as a gatekeeper of synaptic information transfer. *Neural Comput.* **2007**, *19*, 303–326. [[CrossRef](#)] [[PubMed](#)]
75. Valenza, G.; Poggio, G.; Armato, A.; Ferro, M.; Scilingo, E.P.; de Rossi, D. A neuron–astrocyte transistor-like model for neuromorphic dressed neurons. *Neural Netw.* **2011**, *24*, 679–685. [[CrossRef](#)] [[PubMed](#)]
76. Koch, C.; Segev, I. *Methods in Neuronal Modeling*; Massachusetts Institute of Technology: Cambridge, MA, USA, 1998; ISBN 0-262-11231-0.
77. Izhikevich, E.M. *Dynamical Systems in Neuroscience: The Geometry of Excitability and Bursting*; Computational Neuroscience; MIT Press: Cambridge, MA, USA, 2006.
78. Gerstner, W.; Brette, R. Adaptive exponential integrate-and-fire model. *Scholarpedia* **2009**, *4*, 8427. [[CrossRef](#)]
79. Pearson, M.J.; Pipe, A.G.; Mitchinson, B.; Gurney, K.; Melhuish, C.; Gilhespy, I.; Nibouche, M. Implementing spiking neural networks for real-time signal-processing and control applications: A model-validated FPGA approach. *IEEE Trans. Neural Netw.* **2007**, *18*, 1472–1487. [[CrossRef](#)] [[PubMed](#)]
80. FitzHugh, R. Impulses and physiological states in theoretical models of nerve membrane. *Biophys. J.* **1961**, *1*, 445–466. [[CrossRef](#)]
81. Morris, C.; Lecar, H. Voltage oscillations in the barnacle giant muscle fiber. *Biophys. J.* **1981**, *35*, 193–213. [[CrossRef](#)]
82. Hodgkin, L.; Huxley, A.F. A quantitative description of membrane current and its application to conduction and excitation in nerve. *J. Physiol.* **1952**, *117*, 500–544. [[CrossRef](#)]
83. Hishiki, T.; Torikai, H. A novel rotate-and-fire digital spiking neuron and its neuron-like bifurcations and responses. *IEEE Trans. Neural Netw.* **2011**, *22*, 752–767. [[CrossRef](#)]
84. Kohno, T.; Aihara, K. Digital spiking silicon neuron: Concept and behaviors in GJ-coupled network. In Proceedings of the International Symposium on Artificial Life and Robotics, Beppu, Japan, 25–27 January 2007.
85. Soleimani, H.; Bavandpour, M.; Ahmadi, A.; Abbott, D. Digital implementation of a biological astrocyte model and its application. *IEEE Trans. Neural Netw.* **2014**, *26*, 127–139. [[CrossRef](#)]
86. Soleimani, H.; Drakakis, E.M. An efficient and reconfigurable synchronous neuron model. *IEEE Trans. Circuits Syst. II* **2017**, *6*, 91–95. [[CrossRef](#)]
87. Nazari, S.; Faez, K.; Karimi, E.; Amiri, M. A digital neuromorphic circuit for a simplified model of astrocyte dynamics. *Neurosci. Lett.* **2014**, *582*, 21–26. [[CrossRef](#)] [[PubMed](#)]
88. Nazari, S.; Amiri, M.; Faez, K.; Amiri, M. Multiplierless digital implementation of neuron–astrocyte signalling on FPGA. *Neurocomputing* **2015**, *164*, 281–292. [[CrossRef](#)]
89. Nazari, S.; Faez, K.; Amiri, M.; Karimi, E. A digital implementation of neuron–astrocyte interaction for neuromorphic applications. *Neural Netw.* **2015**, *66*, 79–90. [[CrossRef](#)] [[PubMed](#)]

90. Haghiri, S.; Ahmadi, A.; Saif, M. Complete Neuron-Astrocyte Interaction Model: Digital Multiplierless Design and Networking Mechanism. *IEEE Trans. Biomed. Circuits Syst.* **2017**, *11*, 117–127. [[CrossRef](#)]
91. Gerstner, W.; Kistler, W.M. *Spiking Neuron Models: Single Neurons, Populations, Plasticity*; Cambridge University Press: Cambridge, UK, 2002.
92. Touboul, J.; Brette, R. Dynamics and bifurcations of the adaptive exponential integrate-and-fire model. *Biol. Cybern.* **2008**, *99*, 319–334. [[CrossRef](#)]
93. Postnov, D.E.; Ryazanov, L.S.; Sosnovtsev, O.V. Functional modeling of neural-glia interaction. *BioSystems* **2007**, *89*, 8491. [[CrossRef](#)]
94. Postnov, D.E.; Koreshkov, R.N.; Brazhe, N.A.; Brazhe, A.R.; Sosnovtseva, O.V. Dynamical patterns of calcium signaling in a functional model of neuron–astrocyte networks. *J. Biol. Phys.* **2009**, *35*, 425–445. [[CrossRef](#)]
95. Batista, C.A.S.; Lopes, S.R.; Viana, R.L.; Batista, A.M. Delayed feedback control of bursting synchronization in a scale-free neuronal network. *Neural Netw.* **2010**, *23*, 114–124. [[CrossRef](#)]
96. Li, J.; Katori, Y.; Kohno, T. An FPGA-based silicon neuronal network with selectable excitability silicon neurons. *Front. Neurosci.* **2012**, *6*, 183. [[CrossRef](#)]